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Quantitative EEG Analyses

PATIENT INFORMATION

Name: mansoreh ehsanmehr
Exam#: RawData NrSign EEG - mansoreh e
Age: 45.87
Gender: female
Handedness: right
Eyes: Closed

RECORDING

Date: 11/16/2024
Ref. By:
Test Site:
Analysis Length: 04:53
Ave. SH Reliability: 0.97
Ave. TRT Reliability: 0.97

MEDICATION:

HISTORY:

SUMMARY: The qEEG analyses were deviant from normal and showed dysregulation in bilateral frontal lobes - especially in the left frontal lobe, bilateral temporal lobes - especially in the right temporal lobe, and bilateral parietal lobes - especially in the right parietal lobe. LORETA showed dysregulation in the right occipital lobe, right supramarginal gyrus, and right postcentral gyrus. The frontal lobes are involved in executive functioning, abstract thinking, expressive language, sequential planning, mood control, and social skills. The temporal lobes are involved in auditory information processing, short-term memory, receptive language on the left, and face recognition on the right. The parietal lobes are involved in visual-spatial information processing, short-term memory, executive attention, receptive language on the left, and empathy control and awareness of emotional expression in others on the right (e.g., prosody). The occipital lobes are involved in the visual processing of color, form, movement, visual perception, and spatial processing. The postcentral gyrus is involved with the sense of touch and efferent motor feedback. To the extent there is deviation from normal electrical patterns in these structures, then sub-optimal functioning is expected.

John Doe, Ph.D., QEEG-D, BCIA, ECNS

DETAILED NARRATIVE

LINKED EARS: The Linked Ears power spectral analyses were deviant from normal with excessive power in the right frontal region over a wide frequency range. Excessive power was present in bilateral temporal regions - especially in the right temporal region at 10 Hz and 18 Hz. Excessive power was also present in bilateral parietal regions - especially in the right parietal region over a wide frequency range.

SURFACE LAPLACIAN: The Laplacian power spectral analyses were deviant from normal with excessive power in bilateral frontal regions - especially in the left frontal region over a wide frequency range. Excessive power was present in bilateral temporal regions - especially in the right temporal region over a wide frequency range. Excessive power was also present in bilateral parietal regions - especially in the right parietal region over a wide frequency range.

NEUROIMAGING: LORETA 3-dimensional source analyses were consistent with the surface EEG and showed elevated current sources in the right postcentral gyrus with a maximum at 10 Hz (Brodmann area 1). Elevated LORETA current source also were present in the right supramarginal gyrus with a maximum at 21 Hz (Brodmann area 7). Elevated LORETA current source was present in the right supramarginal gyrus with a maximum at 28 Hz (Brodmann area 7). Elevated LORETA current source was present in the right supramarginal gyrus with a maximum at 29 Hz (Brodmann area 7). Elevated LORETA current source was present in the right occipital lobe with a maximum at 30 Hz (Brodmann area 19).

CONNECTIVITY ANALYSES: EEG amplitude asymmetry, coherence and EEG phase were deviant from normal, especially in frontal, temporal, parietal and occipital relations. Elevated coherence was present in frontal, temporal, parietal and occipital regions which indicates reduced functional differentiation. Reduced coherence was present in frontal, temporal, parietal and occipital regions which indicates reduced functional connectivity. Both conditions are often related to reduced speed and efficiency of information processing.

DISCRIMINANT ANALYSES: The mild head injury discriminant function did not detect a pattern in the EEG that is commonly present in individuals with a history of mild traumatic brain injury.

Concussion Index: The Concussion Index was moderate.

BRAIN FUNCTION INDEX: The Brain Function Index was moderate at 5.92.

NEUROFEEDBACK RECOMMENDATIONS

Surface Neurofeedback: (move towards Z = 0)

FREQ BAND	Delta			Theta			Alpha			Beta1			Beta2			Beta3			High Beta											
FREQ (Hz)	1	2	3	4	5	6	7	8	9	10	11	12	13	14	15	16	17	18	19	20	21	22	23	24	25	26	27	28	29	30
FP1																														
FP2																														
F3																														
F4																														
C3																														
C4																														
P3																														
P4																														
O1																														
O2																														
F7																														
F8																														
T3																														
T4																														
T5																														
T6																														
Fz																														
Cz																														
Pz																														

Coherence Neurofeedback: (move towards Z = 0)

FREQ BAND	Delta			Theta			Alpha			Beta1			Beta2			Beta3			High Beta											
FREQ (Hz)	1	2	3	4	5	6	7	8	9	10	11	12	13	14	15	16	17	18	19	20	21	22	23	24	25	26	27	28	29	30
C3-Cz																														
C3-P3																														
O2-T6																														
F7-T6																														
FP1-T6																														
C3-Pz																														
P4-Pz																														
P4-T6																														
C3-P4																														
Fz-Cz																														

Loreta Neurofeedback: (move towards Z = 0)

FREQ BAND	L	Delta			Theta			Alpha			Beta1			Beta2			Beta3			High Beta											
FREQ (Hz)	R	1	2	3	4	5	6	7	8	9	10	11	12	13	14	15	16	17	18	19	20	21	22	23	24	25	26	27	28	29	30
BA1	R																														
BA7	R																														
BA5	R																														
BA40	R																														
BA3	R																														
BA4	R																														
BA2	R																														
BA39	R																														
BA45	R																														
BA7	L																														
BA46	R																														
BA1	L																														
BA9	R																														
BA5	L																														
BA6	R																														
BA45	L																														
BA46	L																														
BA47	L																														
BA3	L																														
BA4	L																														

The implications for neurotherapy are offered based upon the clinical evaluation of the patient as well as the reference data base results. These suggestions for neurotherapy should be evaluated with caution and should only be considered as possible strategies that the clinician may have considered in his/her evaluation. If the patient is depressed, then the clinician should consider treating this condition first through alpha frequency enhancement or some other biofeedback protocol that may reduce depression. If depression or poor mood and/or motivation is not a problem then the clinician may consider using one or more strategies with the priority of treatment in the order presented above.

Addiction/Reward Network

Surface Neurofeedback: (move towards $Z = 0$)

[illegible]

Coherence Neurofeedback: (move towards $Z = 0$)

Confronting Neural Oscillations (move towards 2%)																														
FREQ BAND	Delta				Theta				Alpha				Beta1				Beta2				Beta3				High Beta					
FREQ (Hz)	1	2	3	4	5	6	7	8	9	10	11	12	13	14	15	16	17	18	19	20	21	22	23	24	25	26	27	28	29	30
C3-Cz																														
Fz-Cz																														
F3-Cz																														
C3-C4																														
C4-Fz																														
C3-F7																														
F3-C4																														
F4-C4																														
F3-C3																														
F4-Fz																														

Loreta Neurofeedback: (move towards $Z = 0$)

[illegible]

Anxiety Network

Surface Neurofeedback: (move towards $Z = 0$)

[illegible]

Coherence Neurofeedback: (move towards $Z = 0$)

Conference Neurofeedback: (move towards 2 – 6)																															
FREQ (Band)	<u>Delta</u>			<u>Theta</u>			<u>Alpha</u>			<u>Beta1</u>		<u>Beta2</u>		<u>Beta3</u>						<u>High Beta</u>											
FREQ (Hz)	1	2	3	4	5	6	7	8	9	10	11	12	13	14	15	16	17	18	19	20	21	22	23	24	25	26	27	28	29	30	
C3-Cz																															
Fz-Cz																															
F3-Cz																															
C3-C4																															
C4-Fz																															
F3-C4																															
F4-C4																															
F3-C3																															
F4-Fz																															
C4-Cz																															

Loreta Neurofeedback: (move towards $Z = 0$)

[illegible]

Attention Network

Surface Neurofeedback: (move towards $Z = 0$)

[illegible]

Coherence Neurofeedback: (move towards $Z = 0$)

[illegible]

Loreta Neurofeedback: (move towards $Z = 0$)

[illegible]

Default Mode Network

Surface Neurofeedback: (move towards $Z = 0$)

[illegible]

Coherence Neurofeedback: (move towards $Z = 0$)

FREQ BAND	Delta			Theta				Alpha				Beta1				Beta2				Beta3						High Beta				
FREQ (Hz)	1	2	3	4	5	6	7	8	9	10	11	12	13	14	15	16	17	18	19	20	21	22	23	24	25	26	27	28	29	30
O2-T6																														
P4-Pz																														
P4-T6																														
Fz-Cz																														
F3-Cz																														
F3-T6																														
T6-Pz																														
P4-O2																														
P3-T6																														
P4-Cz																														

Loreta Neurofeedback: (move towards $Z = 0$)

[illegible]

Mood Network

Surface Neurofeedback: (move towards $Z = 0$)

[illegible]

Coherence Neurofeedback: (move towards $Z = 0$)

[illegible]

Loreta Neurofeedback: (move towards $Z = 0$)

[illegible]

Executive Function Network

Surface Neurofeedback: (move towards $Z = 0$)

[illegible]

Coherence Neurofeedback: (move towards $Z = 0$)

Confronts the wear electrode (moving towards 2°)																														
FREQ BAND	Delta			Theta			Alpha			Beta1			Beta2			Beta3			High Beta											
FREQ (Hz)	1	2	3	4	5	6	7	8	9	10	11	12	13	14	15	16	17	18	19	20	21	22	23	24	25	26	27	28	29	30
C3-Cz																														
C3-P3																														
C3-Pz																														
P4-Pz																														
C3-P4																														
Fz-Cz																														
F3-Cz																														
C3-C4																														
C4-P4																														
C4-Fz																														

Loreta Neurofeedback: (move towards $Z = 0$)

[illegible]

Memory Network

Surface Neurofeedback: (move towards $Z = 0$)

[illegible]

Coherence Neurofeedback: (move towards $Z = 0$)

CONFERENCE HEAD PRESENTATION (minutes towards 2:00)																														
FREQ BAND	Delta				Theta				Alpha				Beta1				Beta2				Beta3				High Beta					
FREQ (Hz)	1	2	3	4	5	6	7	8	9	10	11	12	13	14	15	16	17	18	19	20	21	22	23	24	25	26	27	28	29	30
T3-T5																														
T4-T6																														
T3-T4																														
T4-T5																														
T5-T6																														

Loreta Neurofeedback: (move towards $Z = 0$)

[illegible]

Pain Network

Surface Neurofeedback: (move towards $Z = 0$)

[illegible]

Coherence Neurofeedback: (move towards $Z = 0$)

[illegible]

Loreta Neurofeedback: (move towards $Z = 0$)

[illegible]

Mirror Neuron Network

Surface Neurofeedback: (move towards $Z = 0$)

[illegible]

Coherence Neurofeedback: (move towards $Z = 0$)

Conferencing Near electrode (move towards 2°)																														
FREQ BAND	Delta			Theta			Alpha			Beta1			Beta2			Beta3			High Beta											
FREQ (Hz)	1	2	3	4	5	6	7	8	9	10	11	12	13	14	15	16	17	18	19	20	21	22	23	24	25	26	27	28	29	30
C3-Cz																														
Fz-Cz																														
F7-T3																														
C3-C4																														
C4-Fz																														
C3-F7																														
C3-T3																														
T4-Cz																														
T3-T4																														
T3-Fz																														

Loreta Neurofeedback: (move towards $Z = 0$)

[illegible]

Salience Network

Surface Neurofeedback: (move towards $Z = 0$)

[illegible]

Coherence Neurofeedback: (move towards $Z = 0$)

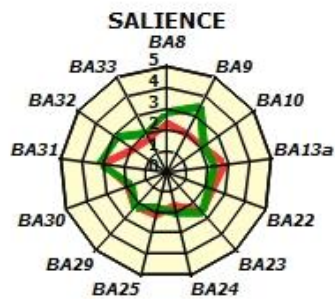
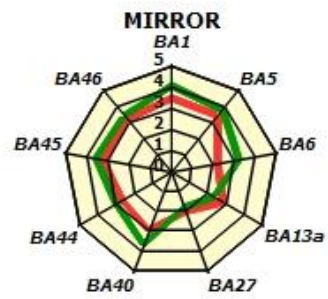
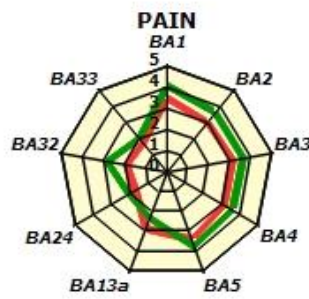
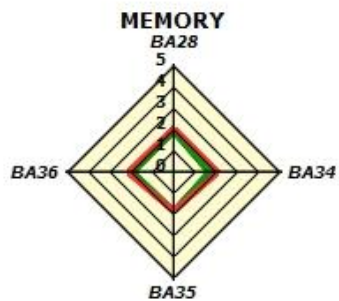
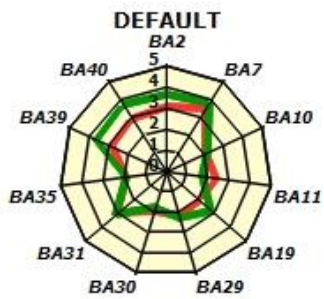
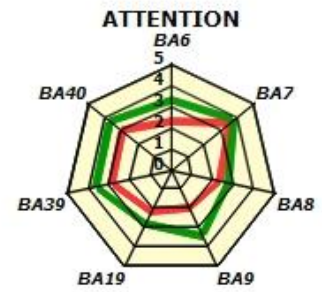
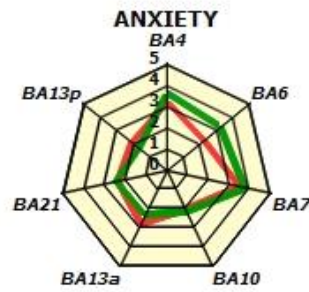
[illegible]

Loreta Neurofeedback: (move towards $Z = 0$)

[illegible]

NETWORK zSCOREs

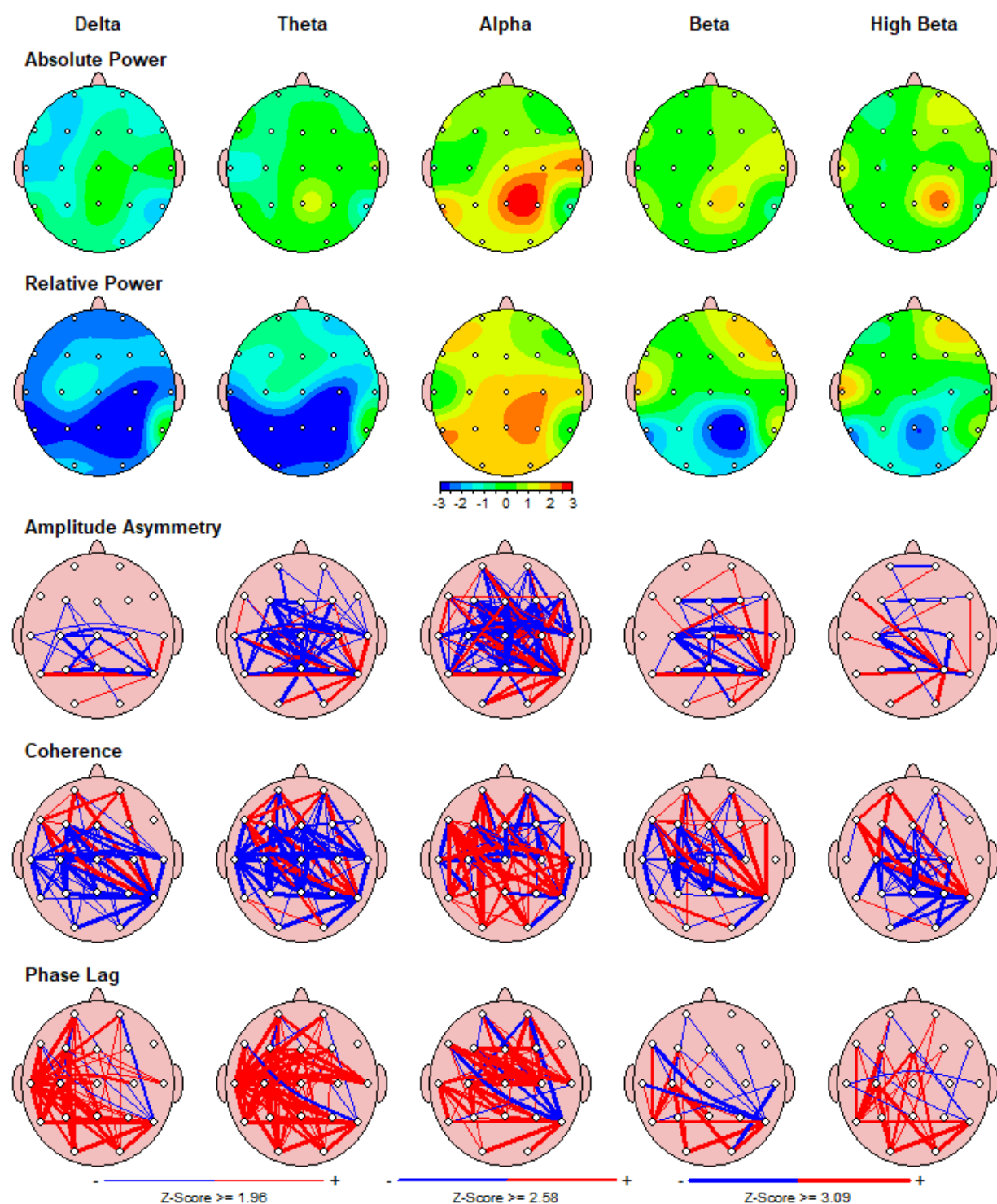
(Circles = zSCOREs, Radial Lines = Brodmann Areas)



LEFT RIGHT

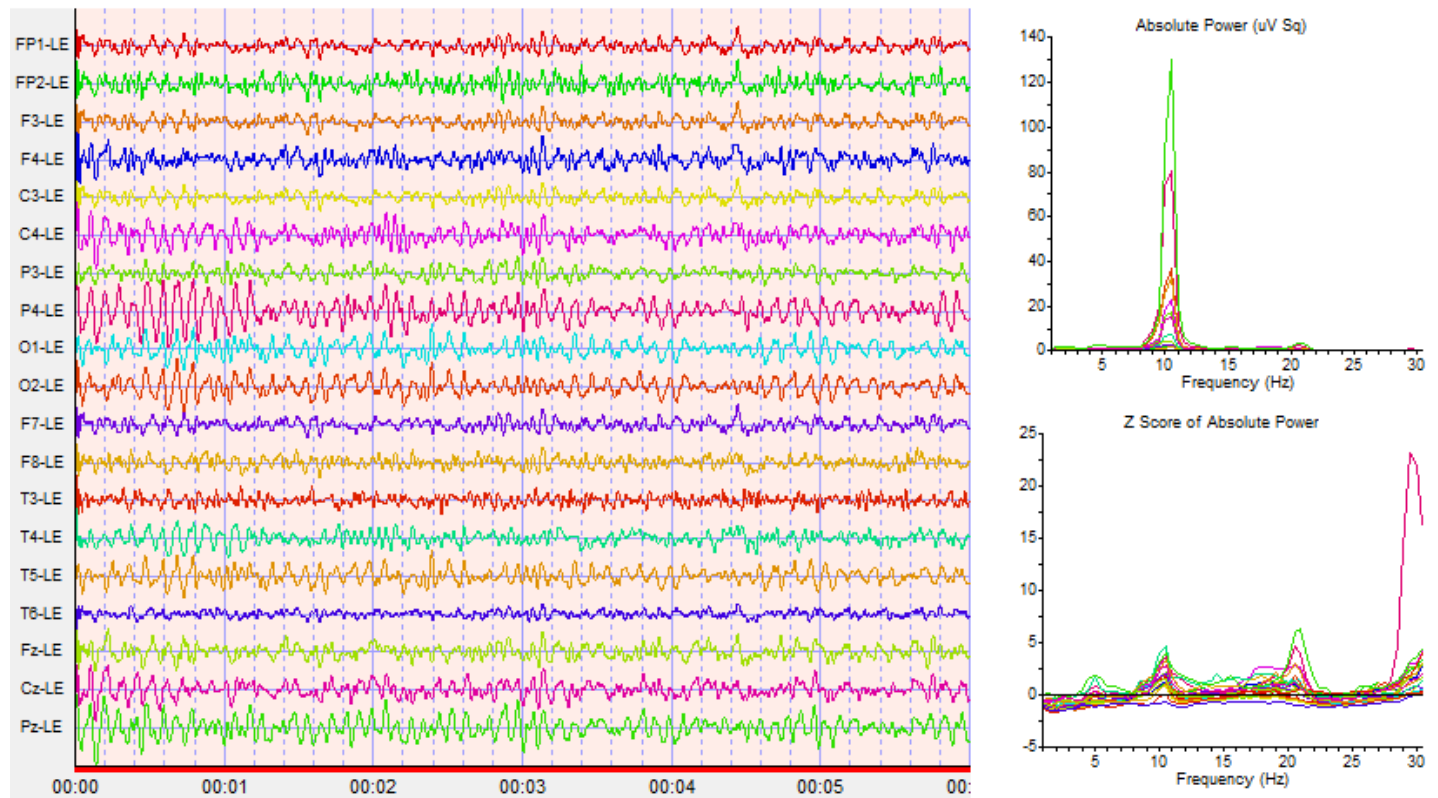
Montage: LinkEEEG ID: RawData NrSign EEG - mansoreh ehsanmehr Saturday, November 16, 2024 5_14_06 PM - 202

Z Scored FFT Summary Information

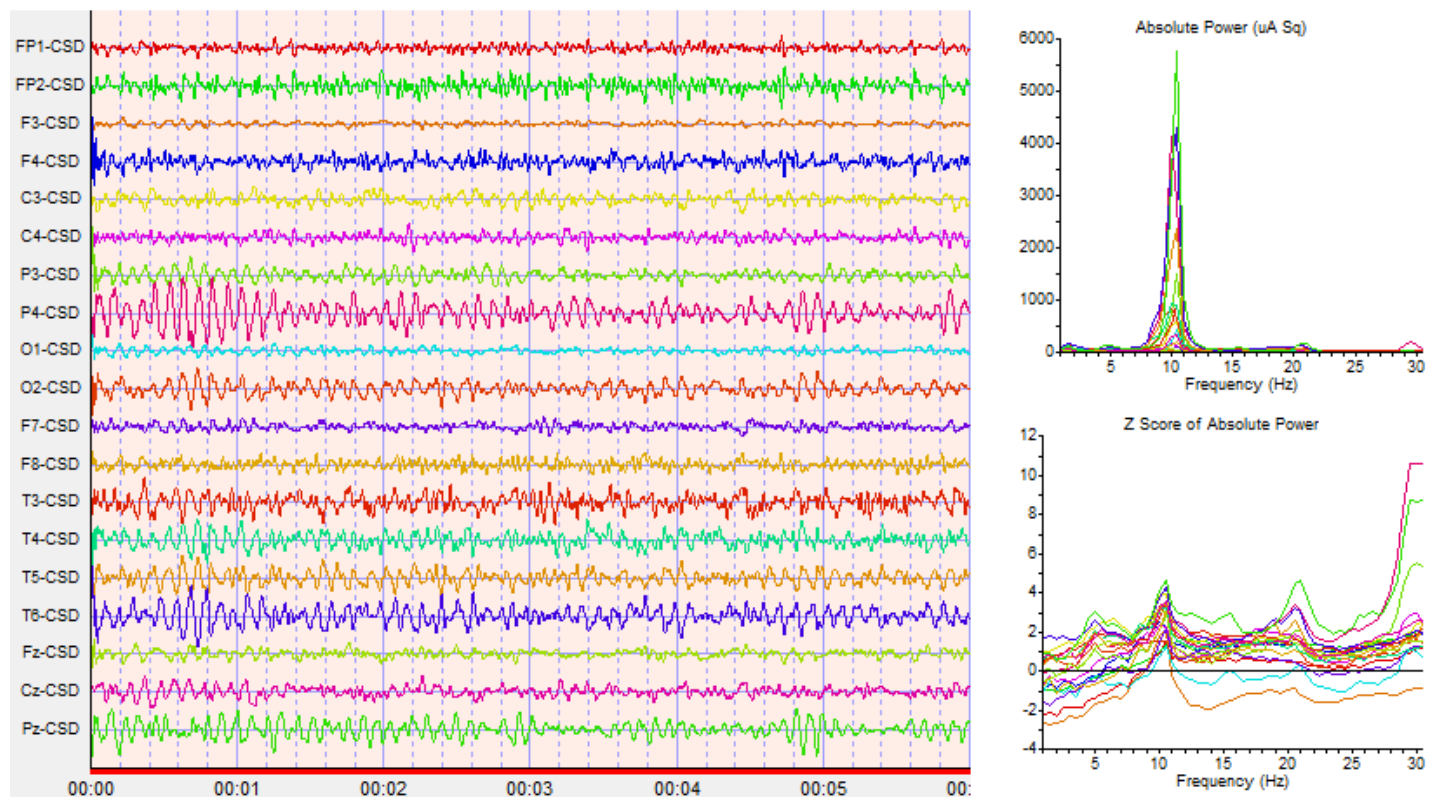


Conventional EEG Samples and Quantitative EEG Analyses

Example of Linked Ears EEG and Absolute Power - Eyes Closed Condition



Example of Laplacian EEG and Absolute Power - Eyes Closed Condition



Electrical NeuroImaging

Linking a patient's symptoms and complaints to functional systems in the brain is important in evaluating the health and efficiency of cognitive and perceptual functions. The electrical rhythms in the EEG arise from many sources but approximately 50% of the power arises directly beneath each recording electrode. Electrical NeuroImaging uses a mathematical method called an "Inverse Solution" to accurately estimate the sources of the scalp EEG (Pascual-Marqui et al, 1994; Pascual-Marqui, 1999). Below is a Brodmann map of anatomical brain regions that lie near to each 10/20 scalp electrode with associated functions as evidenced by fMRI, EEG/MEG and PET NeuroImaging methods.

Symptoms, Electrodes & Brodmann Areas

Frontal Lobe (Fp1/Fp2, F3/F4, F7/F8, C3/C4)
Thinking, Planning, Motor Execution, Executive Functions, Mood Control

Temporal Lobe (T3/T5)
Language Function and Auditory Perception
Involved in Long Term Memory and Emotion

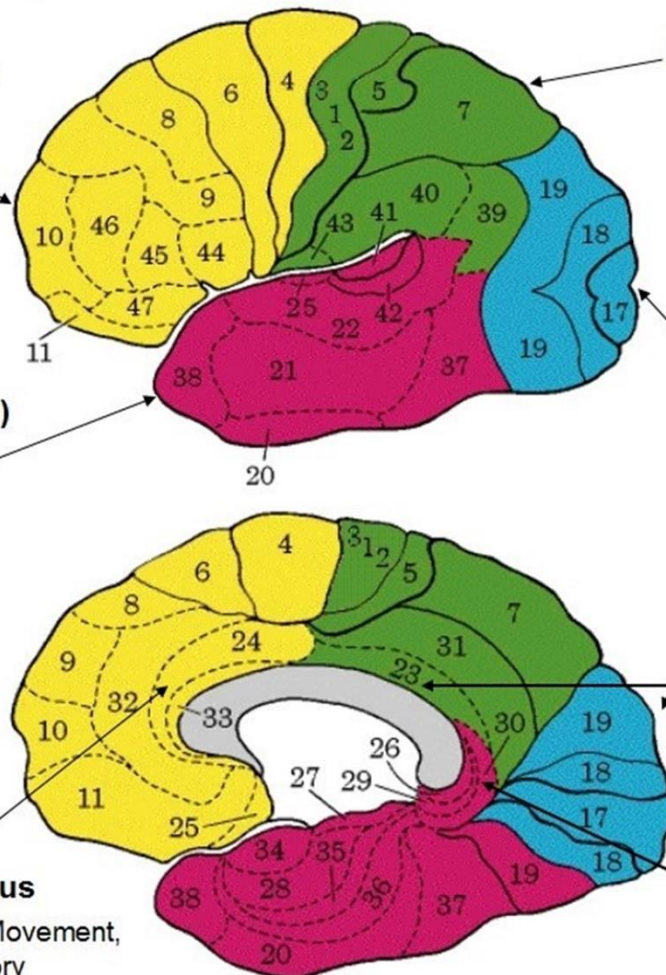
Anterior Cingulate Gyrus (Fz, Cz, C3/C4) Volitional Movement, Attention, Long Term Memory

Parietal Lobe (P3/P4, Pz)
Somatosensory Perception
Integration of Visual and Somatospatial Information

Occipital Lobe (O1/O2, T5/T6)
Visual Perception & Spatial Processing

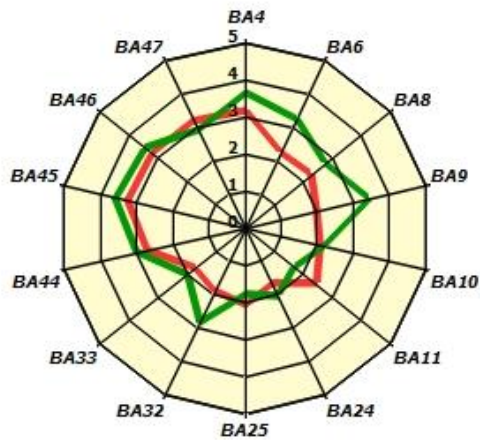
Posterior Cingulate (P3/P4, Pz) Attention, Long-term Memory

Parahippocampal Gyrus (P3/P4, T5/T6, Pz)
Short-term Memory, Attention

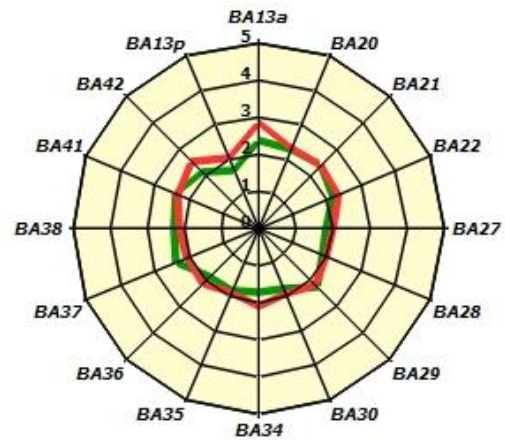


BRAIN BRODMANN REGIONS

FRONTAL BRODMANN AREAS

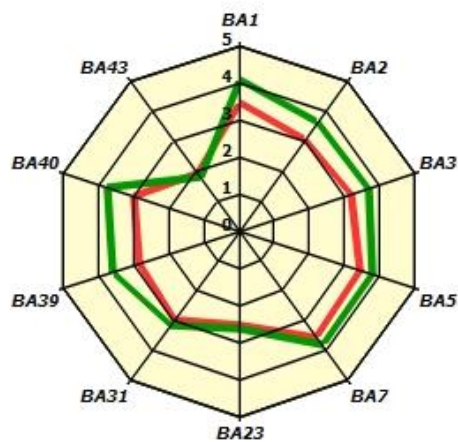


TEMPORAL BRODMANN AREAS

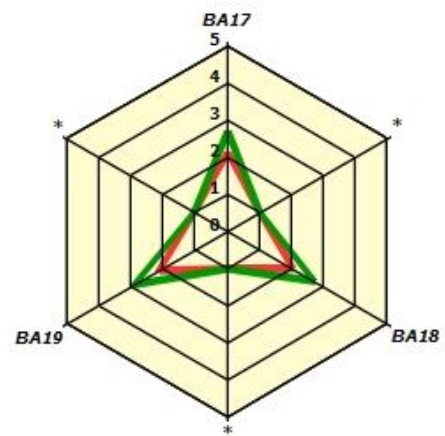


■ LEFT ■ RIGHT

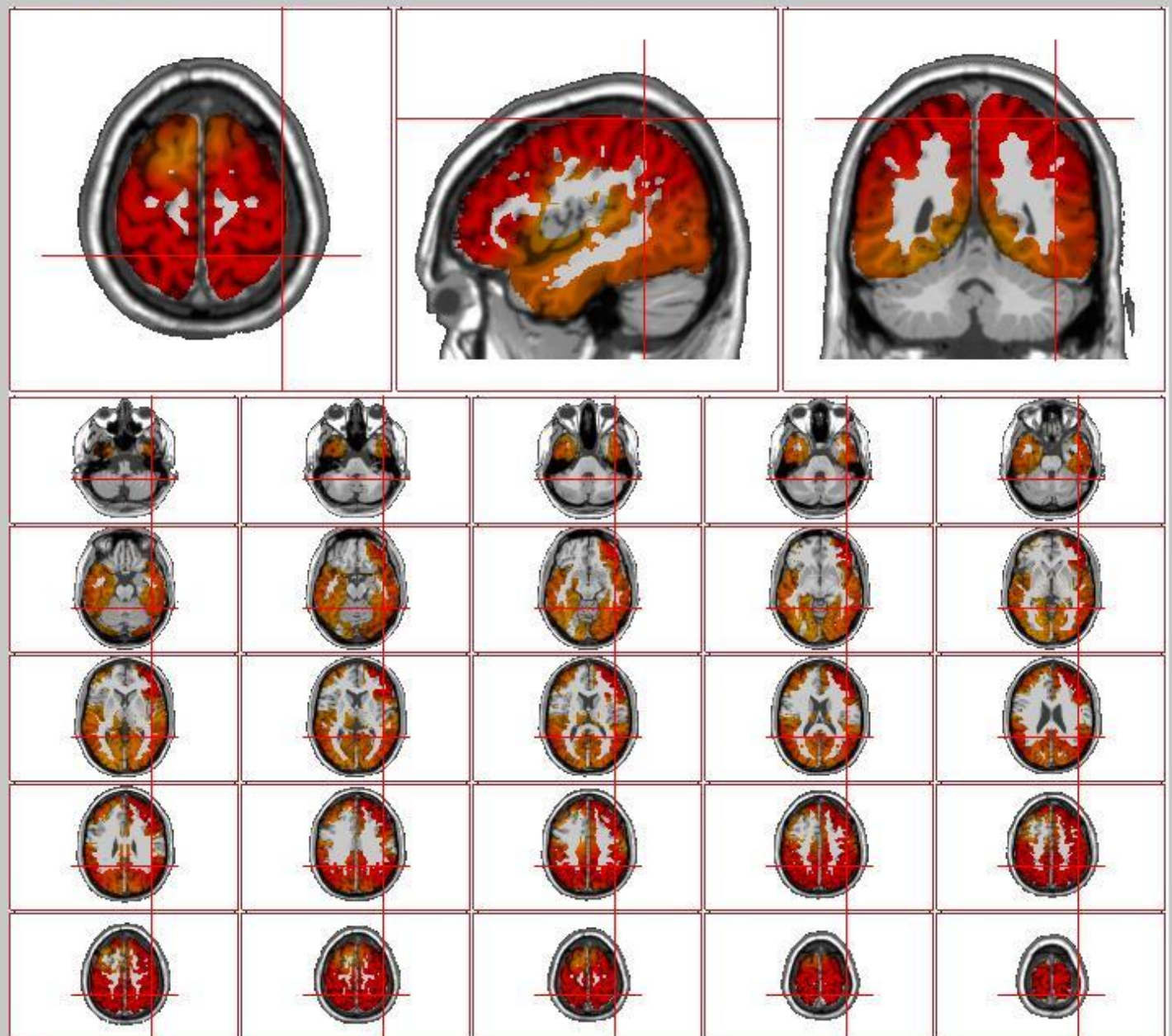
PARIETAL BRODMANN AREAS



OCCIPITAL BRODMANN AREAS

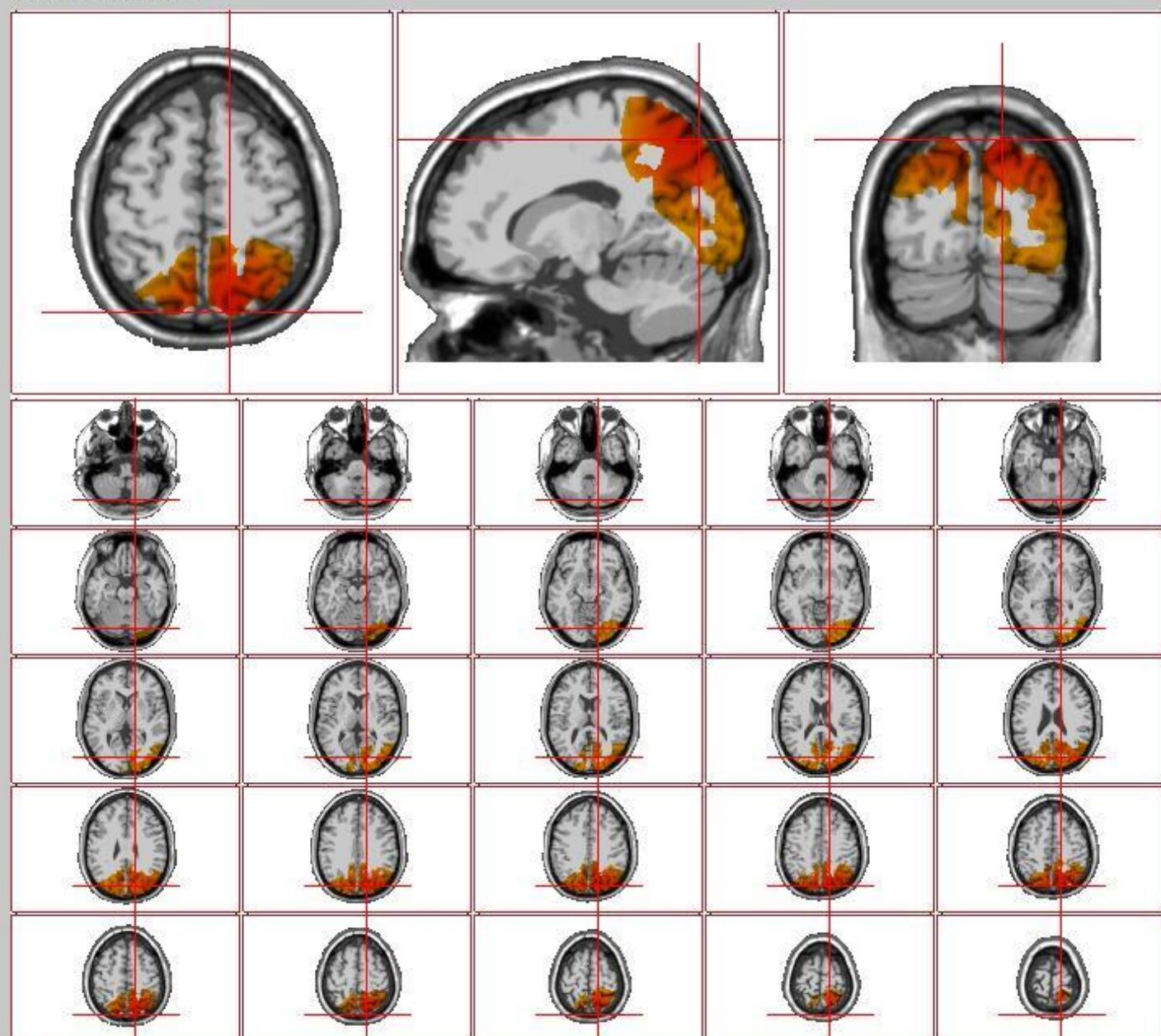


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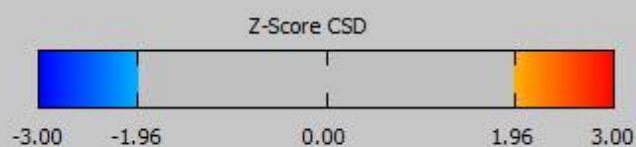


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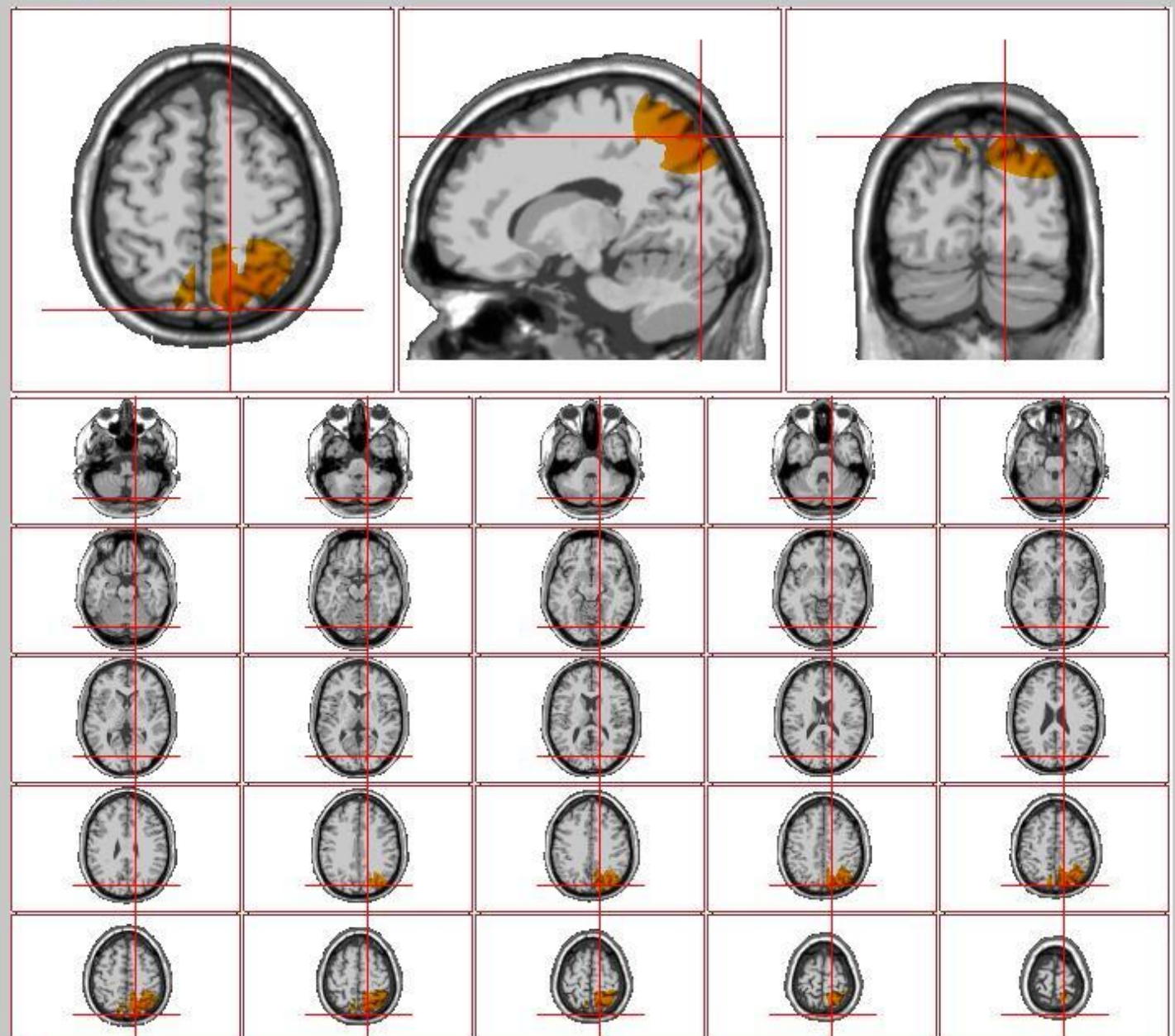
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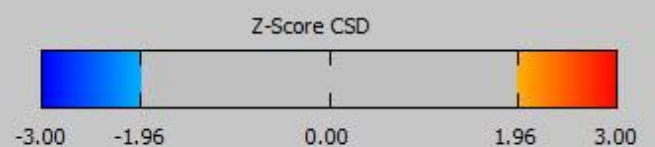
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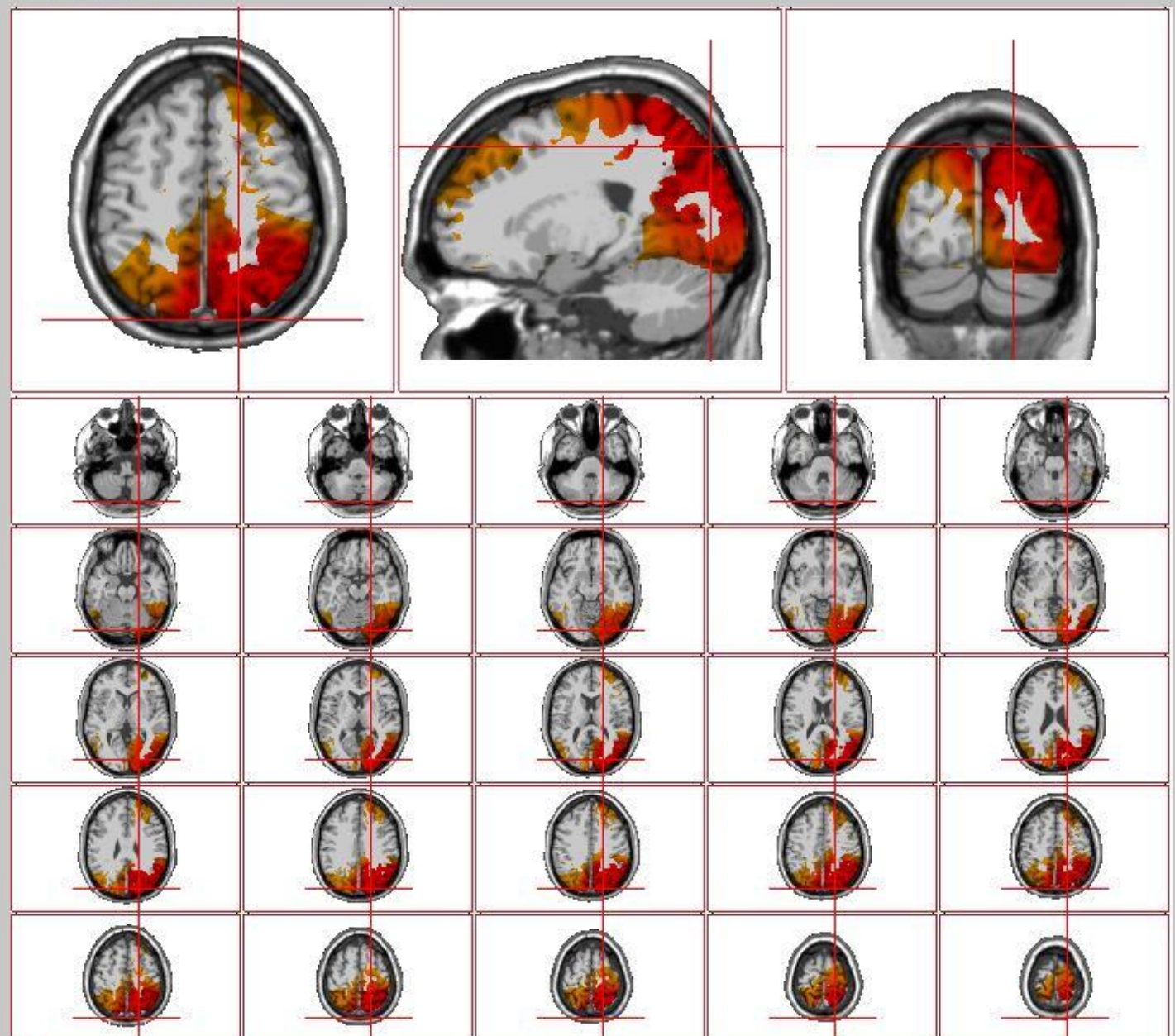
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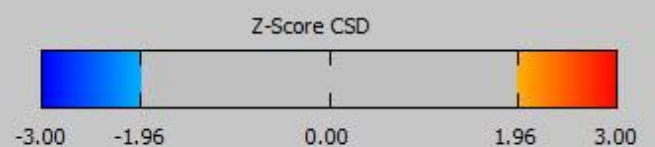
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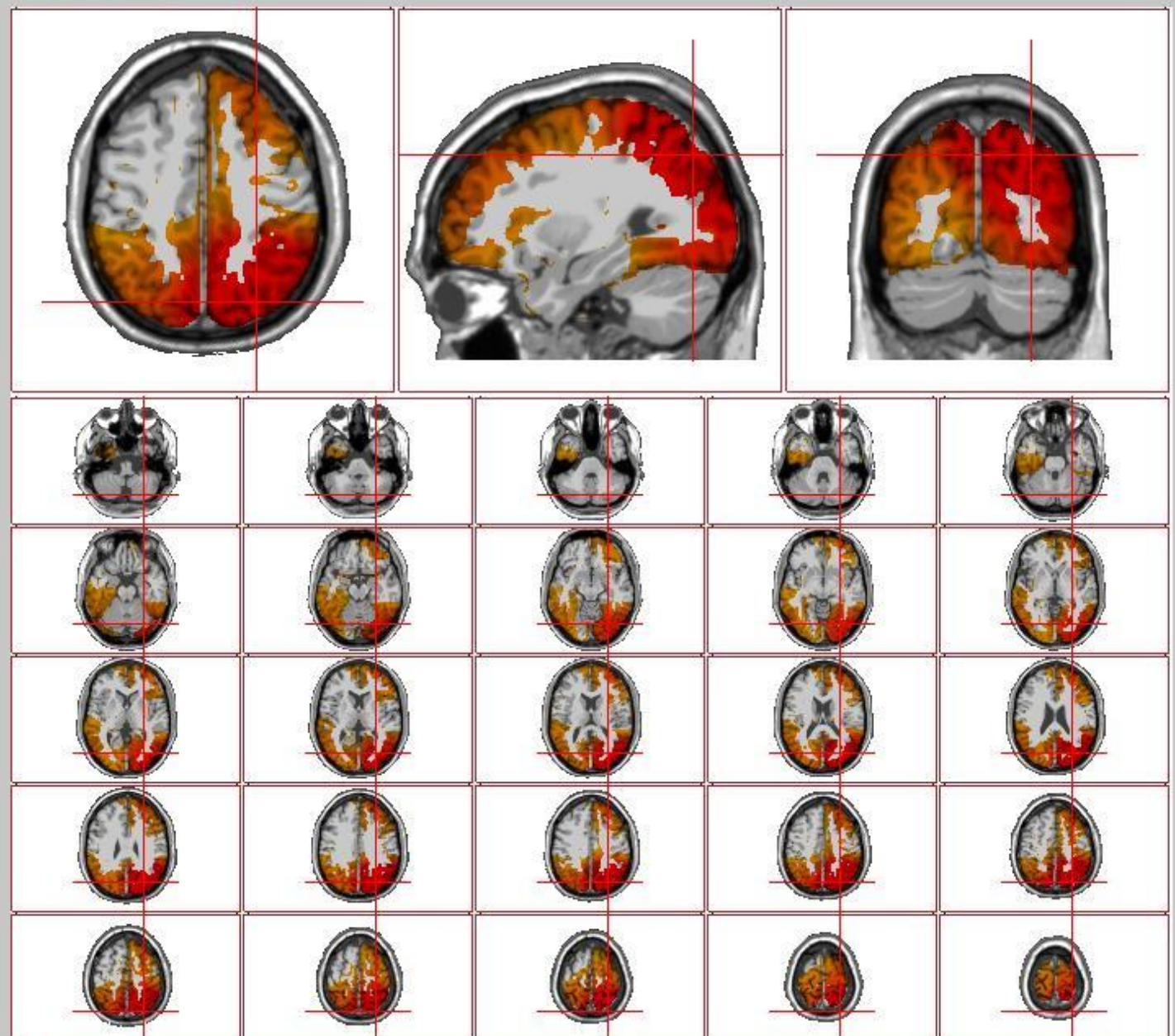
Value = 4.15512 - 29 Hz



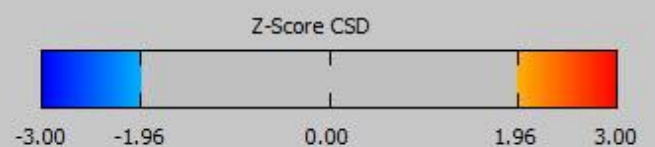
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Value = 4.14405 - 30 Hz

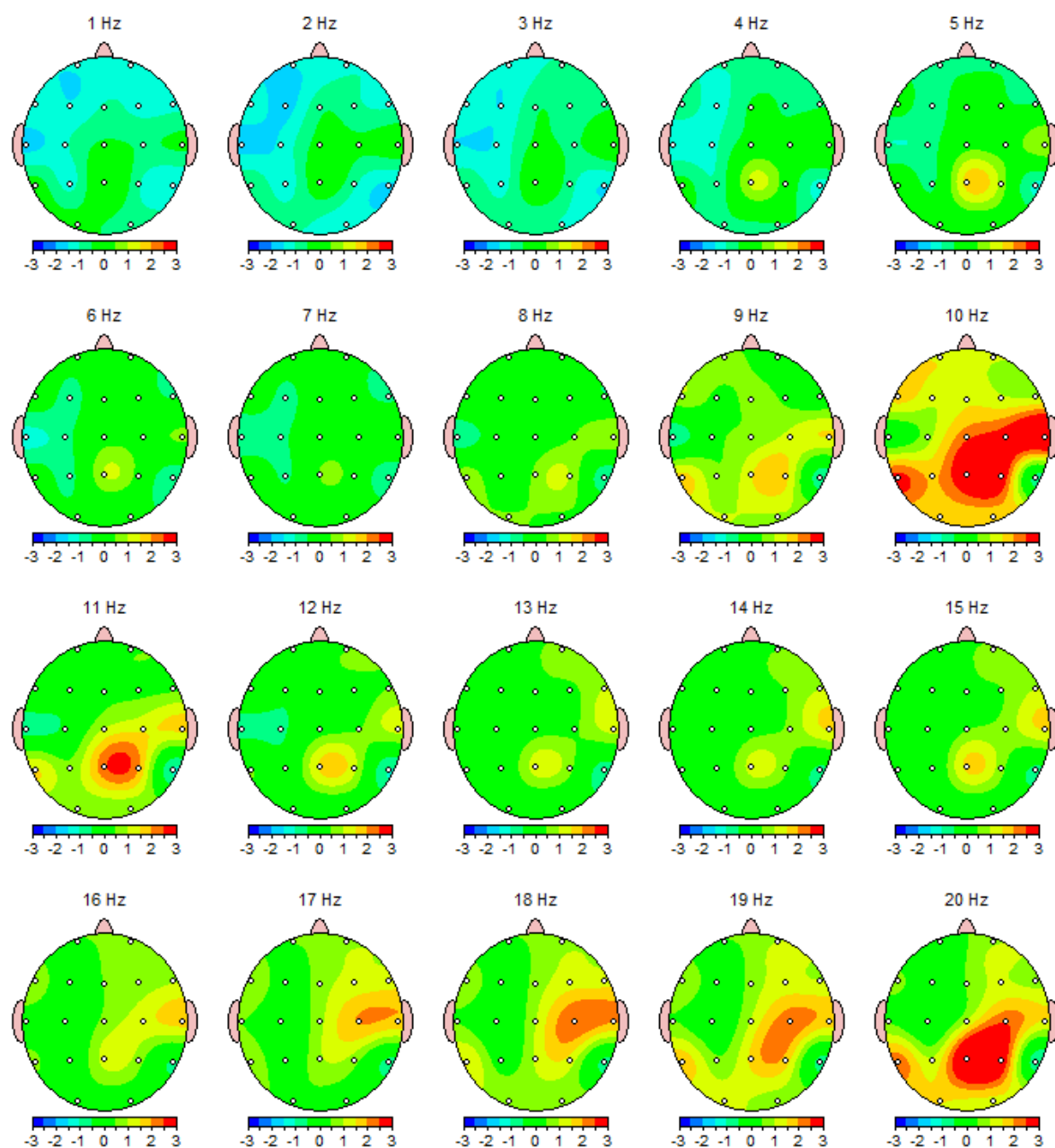


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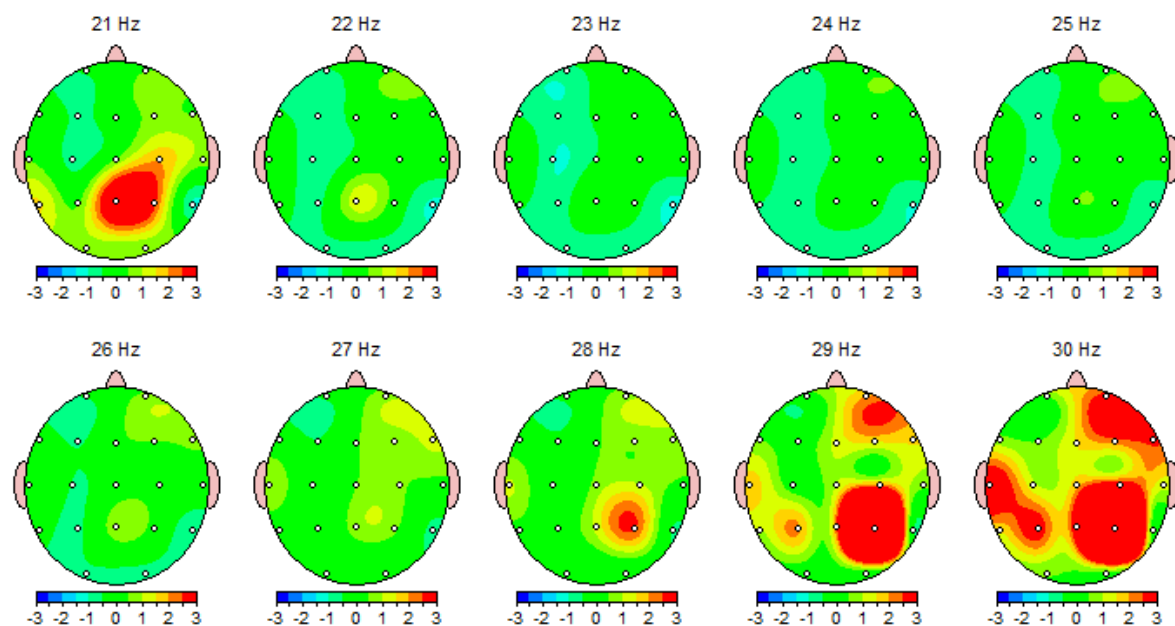


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Z Scored FFT Absolute Power

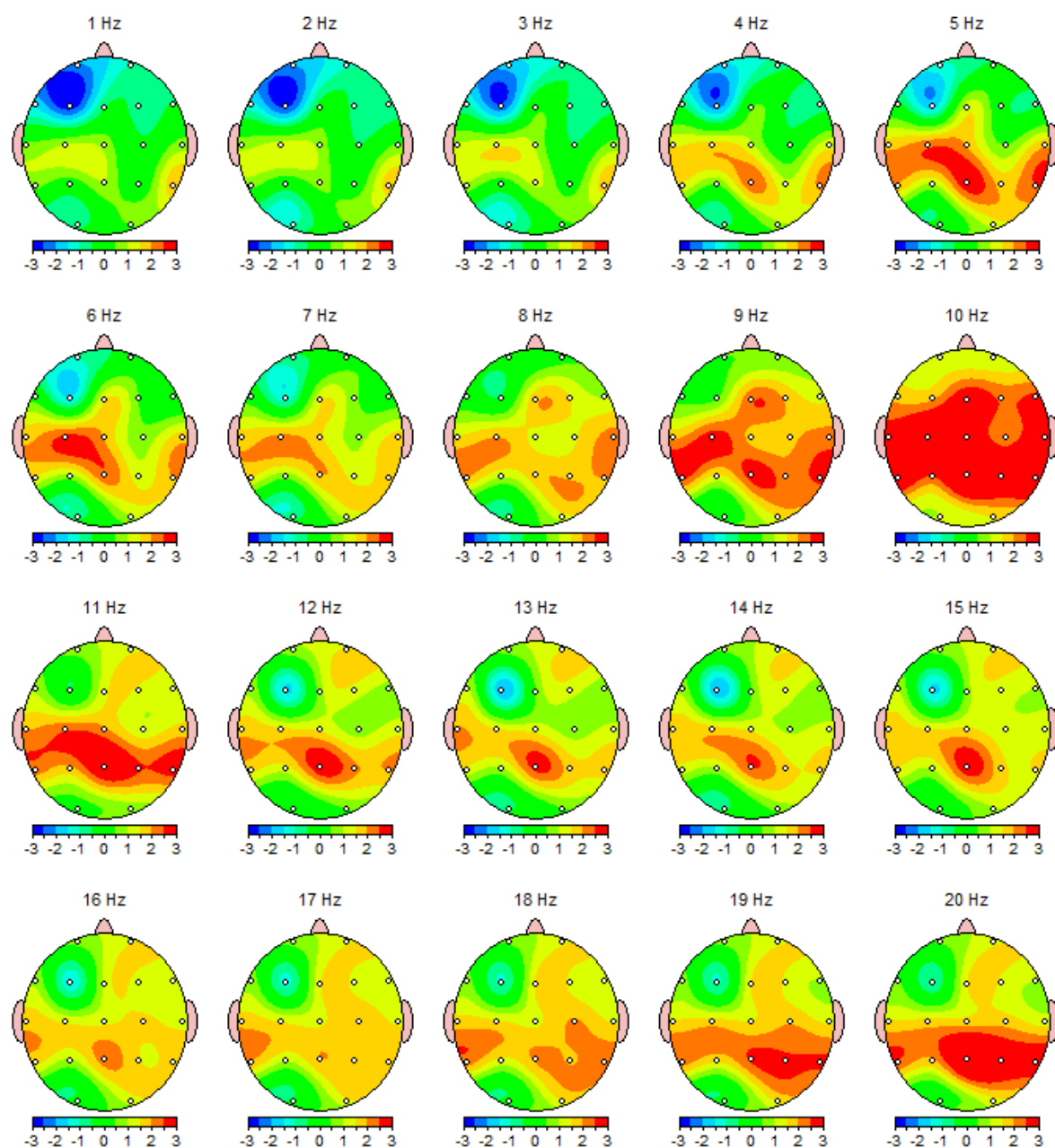


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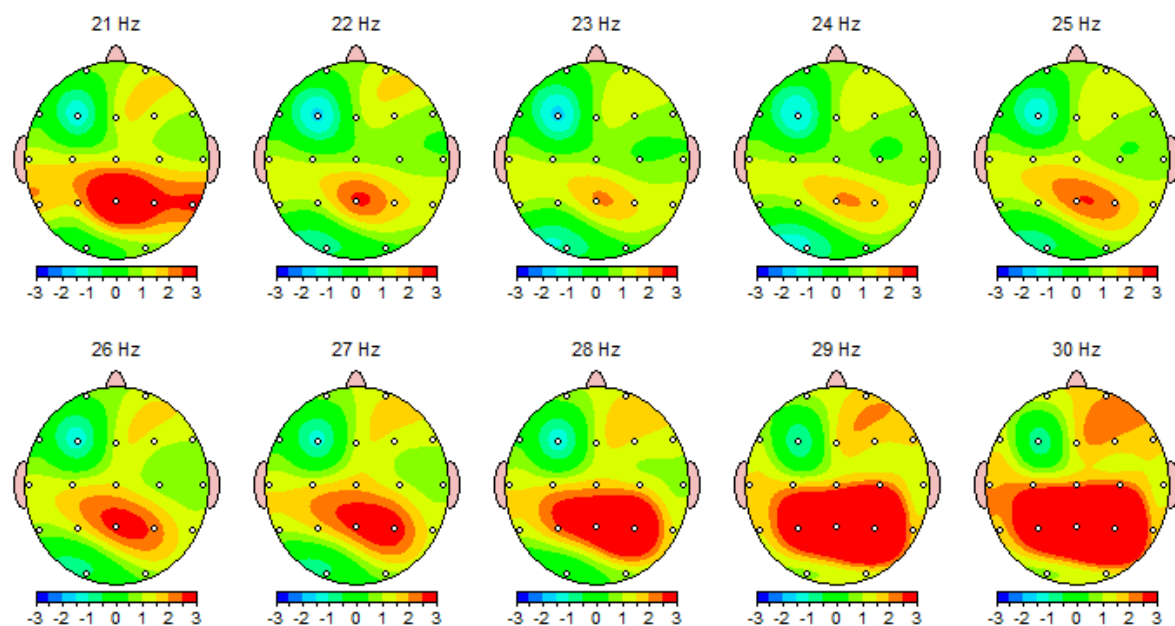
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Z Scored FFT Absolute Power

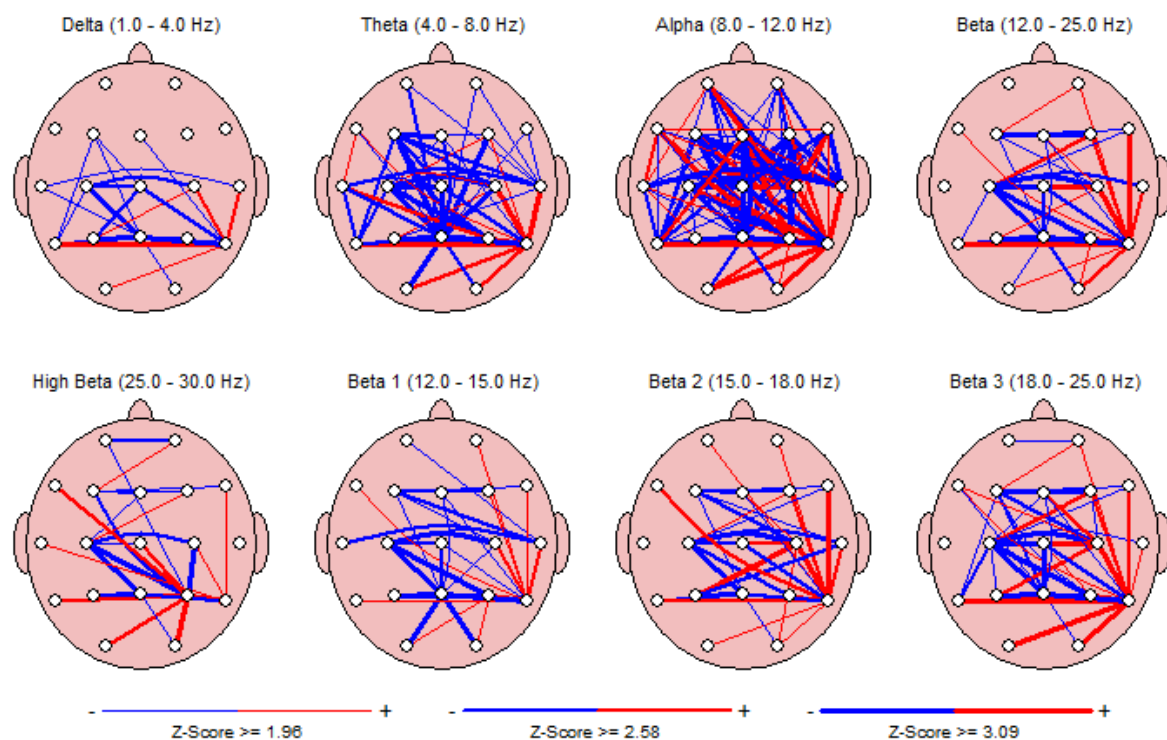


Montage: Laplacian EEG ID: RawData NrSign EEG - mansoreh ehsanmehr Saturday, November 16, 2024 5_14_06 PM - 202

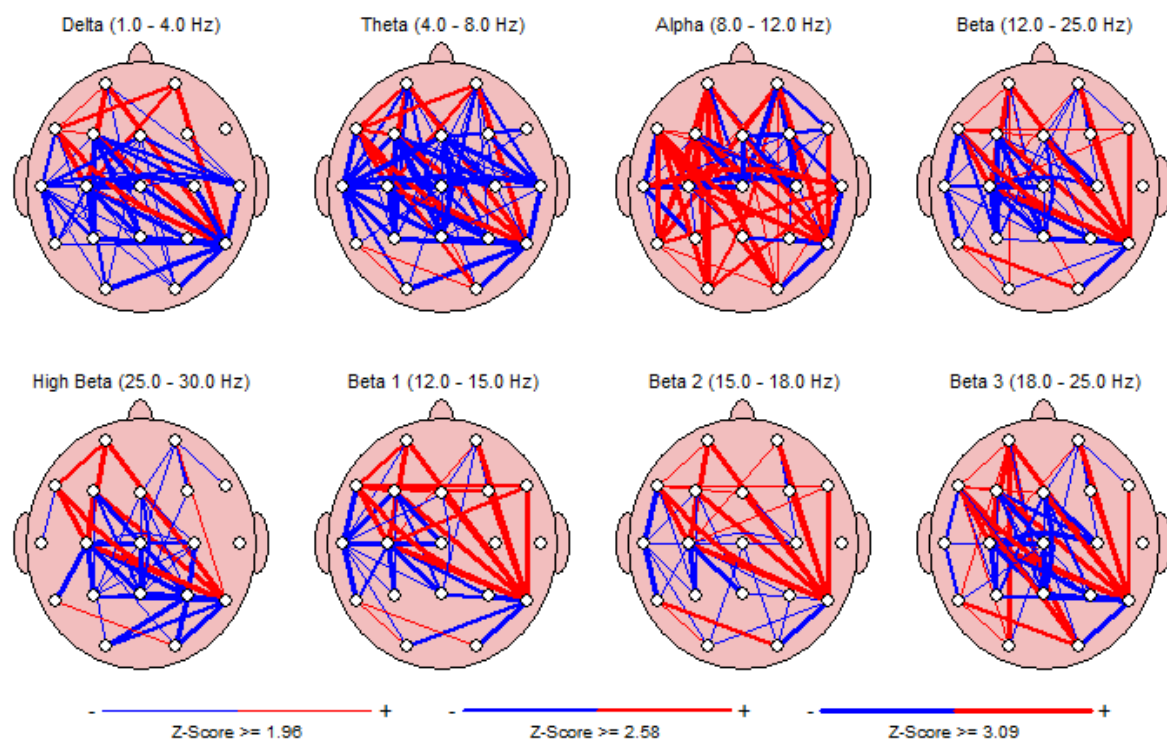
Z Scored FFT Absolute Power



Montage: LinkEEEG ID: RawData NrSign EEG - mansoreh ehsanmehr Saturday, November 16, 2024 5_14_06 PM - 202

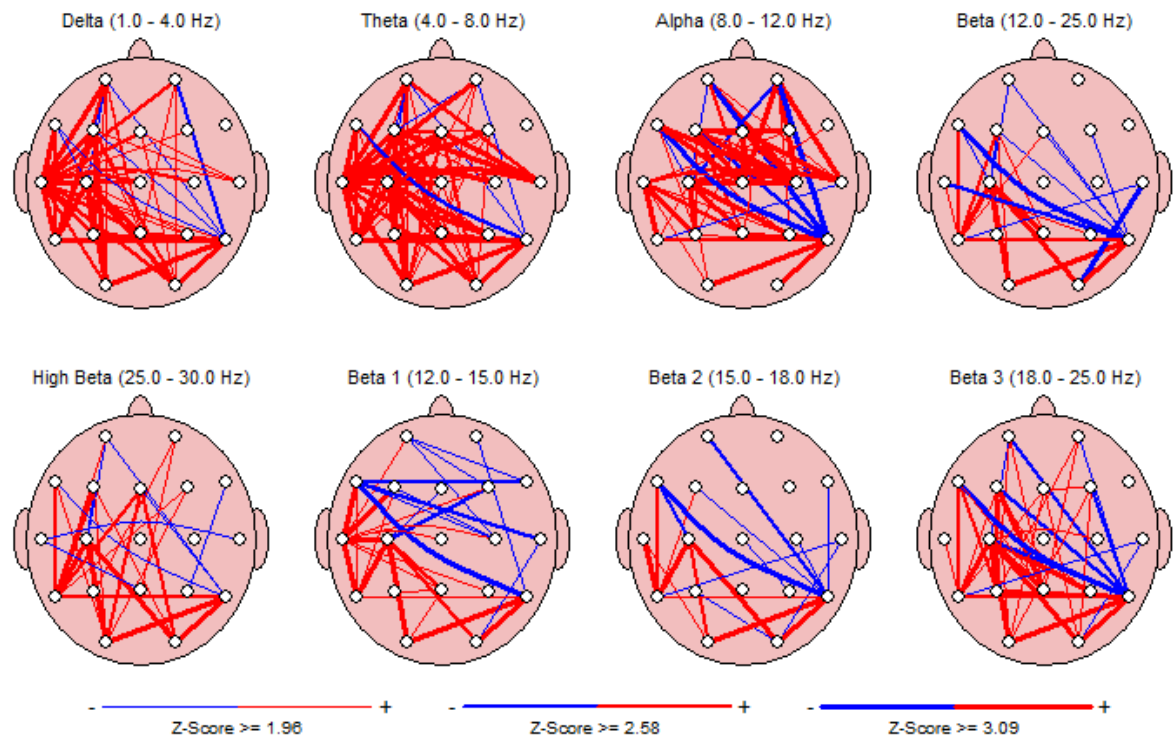
Z Scored FFT Amplitude Asymmetry

Montage: LinkEEEG ID: RawData NrSign EEG - mansoreh ehsanmehr Saturday, November 16, 2024 5_14_06 PM - 202

Z Scored FFT Coherence

Montage: LinkEEEG ID: RawData NrSign EEG - mansoreh ehsanmehr Saturday, November 16, 2024 5_14_06 PM - 202

Z Scored FFT Phase Lag



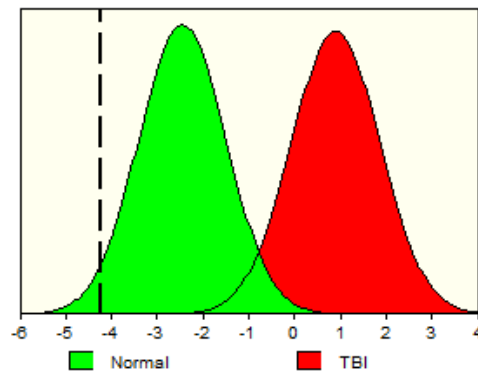
Montage: LinkEEEG ID: RawData NrSign EEG - mansoreh ehsanmehr Saturday, November 16, 2024 5_14_06 PM - 202

Traumatic Brain Injury Discriminant Analysis*

TBI DISCRIMINANT SCORE = -4.26

TBI PROBABILITY INDEX = Not Significant

The TBI Probability Index is the subject's probability of membership in the mild traumatic brain injury population. (see Thatcher et al, EEG and Clin. Neurophysiol., 73: 93-106, 1989.)

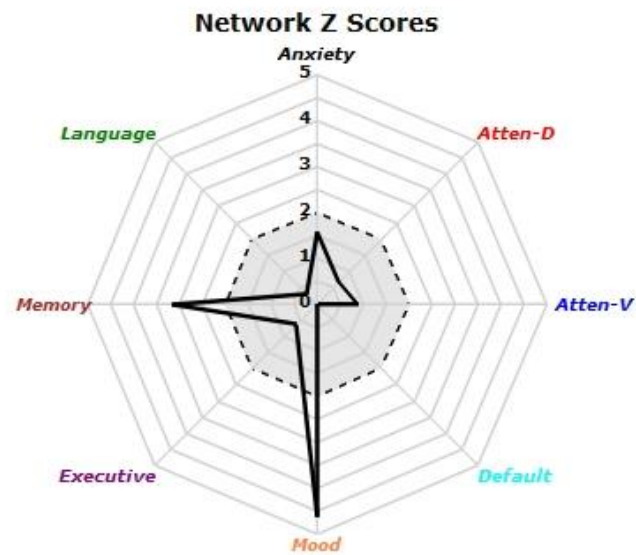
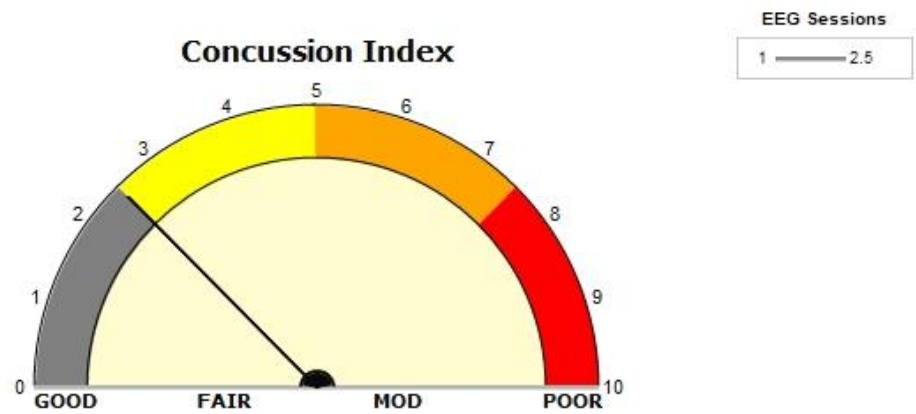


			RAW	Z
FP1-F3	COH	Theta	99.99	2.42
T3-T5	COH	Beta	4.99	-3.16
C3-P3	COH	Beta	5.36	-13.97
FP2-F4	PHA	Beta	0.74	0.59
F3-F4	PHA	Beta	0.18	-0.72
F4-T6	AMP	Alpha	114.20	3.10
F8-T6	AMP	Alpha	59.00	3.02
F4-T6	AMP	Beta	103.83	3.34
F8-T6	AMP	Beta	73.84	3.69
F3-O1	AMP	Alpha	-150.80	-1.58
F4-O2	AMP	Alpha	-147.29	-1.21
F7-O1	AMP	Alpha	150.84	0.91
F4-O2	AMP	Beta	-23.23	0.05
P3	RP	Alpha	73.40	1.33
P4	RP	Alpha	83.93	2.10
O1	RP	Alpha	79.24	1.32
O2	RP	Alpha	81.65	1.36
T4	RP	Alpha	56.49	1.36
T5	RP	Alpha	79.41	2.03
T6	RP	Alpha	38.61	-1.32

***Statement of Indications of Use:**

The Discriminant Analysis and Severity Index are to be used by experienced and qualified professionals for the post-hoc statistical evaluation of the human electroencephalogram (EEG). The Discriminant Analysis and Severity Index are to be viewed as an adjunct to the evaluation of the patient, and they do not serve as a primary basis for a diagnosis. Warning: Inclusion criteria of a history of traumatic brain injury and greater than 13 years of age must be adhered to.

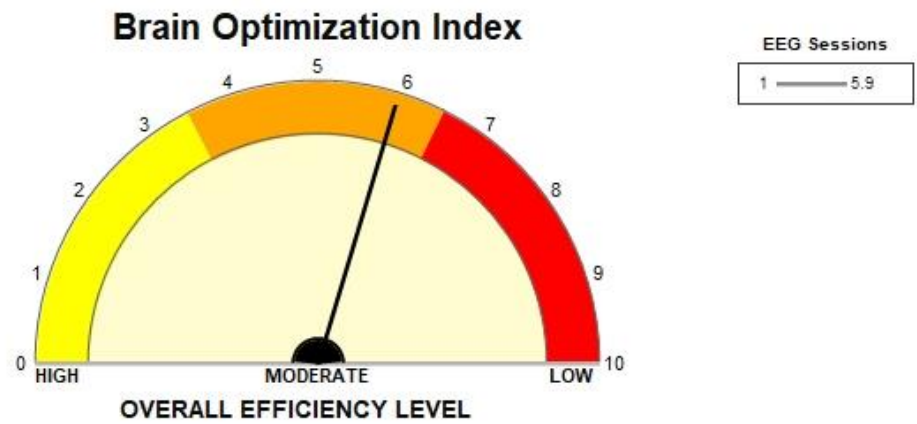
Subject ID: 1285981588



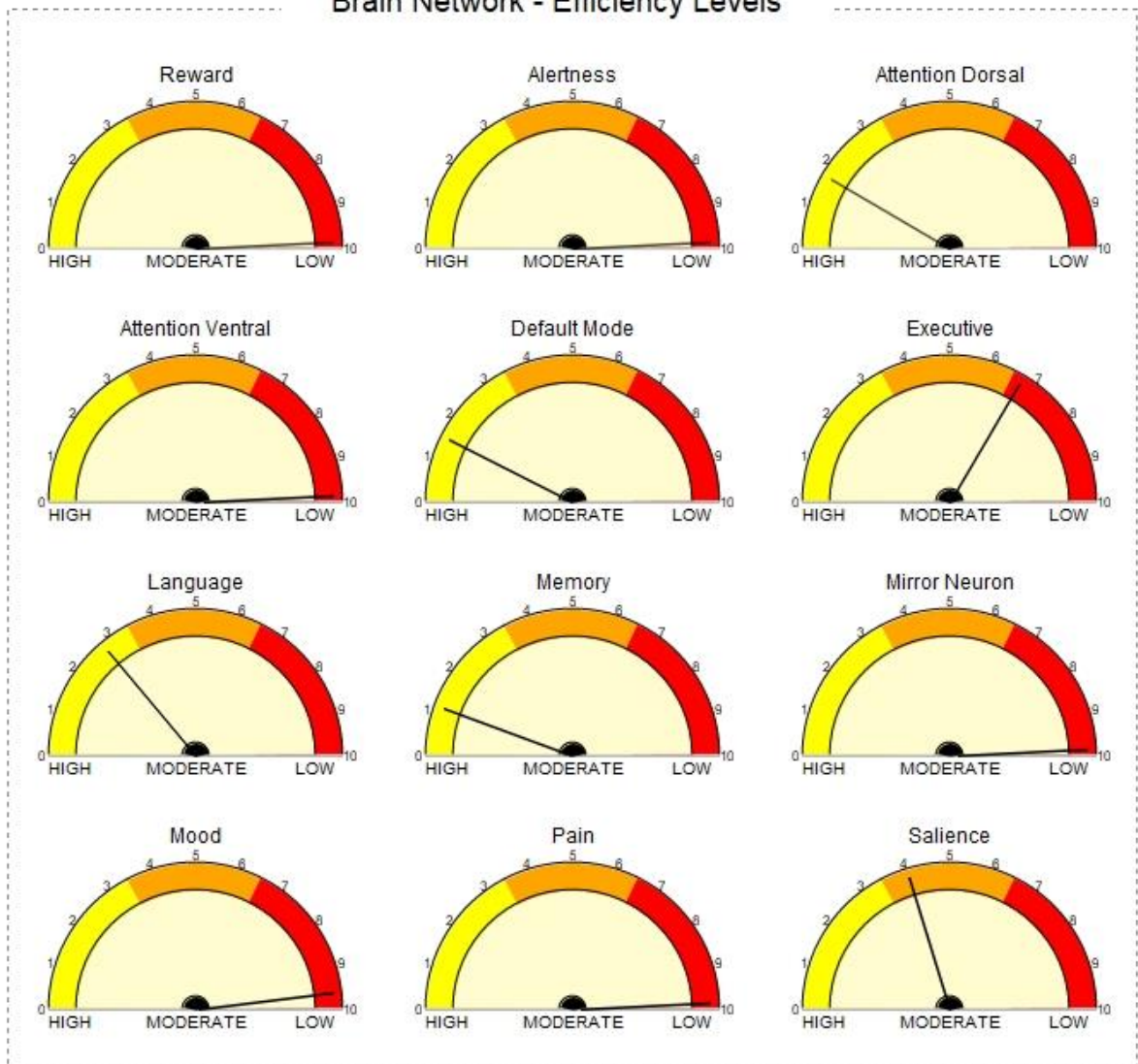
***Statement of Indications of Use:**

The Concussion Index is to be used by experienced and qualified professionals for the post-hoc statistical evaluation of the human electroencephalogram (EEG). The Concussion Index is to be viewed as an adjunct to the evaluation of the patient, and does not serve as a primary basis for a diagnosis.

Subject ID: 1285981588



Brain Network - Efficiency Levels



Montage: LinkEEG ID: RawData NrSign EEG - mansoreh ehsanmehr Saturday, November 16, 2024 5_14_06 PM - 202

Technical Information

Record Length: 04:53

Edit Length: 04:53

Reliability:

	Split Half	Test Retest
Average	0.97	0.97
FP1	0.98	0.97
FP2	0.99	0.98
F3	0.98	0.97
F4	0.98	0.99
C3	0.98	0.97
C4	0.95	0.98
P3	0.94	0.82
P4	0.96	0.83
O1	0.97	0.99
O2	0.97	0.99
F7	0.98	0.97
F8	0.99	0.99
T3	0.99	1.00
T4	1.00	0.98
T5	0.96	0.99
T6	0.98	1.00
Fz	0.99	0.97
Cz	0.96	0.97
Pz	0.94	0.99

Sampling Rate: 500

Collection Hardware: Unknown

An Addendum to NeuroGuide QEEG Report

Important Disclaimer:

QEEG tests are ancillary tests that are not intended to provide a diagnosis by themselves, but are used to evaluate the nature and severity of deregulation in the brain such as in mild traumatic brain injury (MTBI). The QEEG tests provide a quantitative assessment of areas of brain dysfunction and information on impaired conduction and connectivity between different regional neural networks in the brain. The assessment of impaired connectivity is based on abnormal measurements of Coherence and Phase. The TBI Discriminant and Concussion Index do not provide a diagnosis for MTBI but only information on the presence of a pattern in the EEG that is often found in patients with a history of mild traumatic brain injury. The TBI Discriminant and Concussion Index also provide information about connectivity and excitability of brain regions. The TBI Discriminant and Concussion Index are to be used only on patients with a clinical history and symptoms of a Traumatic Brain Injury and Post Concussion syndrome. The diagnosis of MTBI is a clinical one and is not based on any one test. A diagnosis is performed by the clinician, who integrates the medical history, clinical symptoms, neurocognitive tests with the abovementioned brain function tests as well as other information to render a diagnosis. The information on impaired brain connectivity is derived primarily from abnormal measurements of Coherence and Phase. Assessments of regional abnormality rely also on abnormal amplitude (power) distribution across the spectrum of EEG frequencies as compared to the normative database.

Artifact Rejection:

NeuroGuide uses the standard deletion of artifact method to only select artifact free EEG data for analyses. The entire EEG record must be viewed by clicking end and page down and page up and home and by arrow keys and by moving the wiper at the bottom of the screen. A careful visual examination of the EEG record is necessary to detect epilepsy and gross pathology as well as to identify artifacts. The goal is to avoid selecting any artifact and instead to only select artifact free segments of EEG. There are three methods of obtaining Artifact Free Selections: 1- Manual Selections are obtained by pressing the left mouse button and dragging to select, press right mouse button and drag to erase; 2- Artifact Free Template Matching; and 3- Z Score Artifact Free Selections. All three methods can be used and manual selection takes priority over all methods of artifact free selection. That is, left and right mouse button dragging will override all other methods. View the Length of EEG Selections in seconds and View the dynamic Reliability Measures of the EEG Selections. For Manual Selections of Artifact Free EEG Depress the left mouse button and drag it over the sections of EEG that do not contain eye movement or muscle or drowsiness or head movement or any other type of artifact. Select at least 60 seconds of artifact free EEG data as shown in the Edit Time counter (upper left of screen). If a mistake is made, then right mouse click and drag over the EEG traces to erase a selection. View the Test Re-Test reliability which must be at least 0.90. Scan the EEG record and select real and valid EEG and avoid selecting artifact. Splice discontinuities are removed by filtering and exercises to prove no distortion due to splicing are available in the Handbook of QEEG and EEG Biofeedback. Pattern recognition routines are used to identify likely eye movement (EOG), drowsiness and muscle (EMG) artifact in the record and thereby mark these suspected segments and disallow them to be included in subsequent analyses. The pattern recognition routines are based on physics and physiology of artifact. For example, all electrical sources decrement with distance and in the case of eye movement detection is by the presence of an electrical field gradient in the delta frequency band from $Fp1/2 > F3/4 > C3/4$ and/or 120 degrees or higher of inverse phase between F7 and F8. EMG electrical gradients at > 10 Hz from $T3/4 > C3/4$ and/or $Fp1/2$

> F3/4 > C3/4 and/or O1/2 > P3/4. Drowsiness occurs when the locus coeruleus reduces inhibition on the hypothalamic sleep centers resulting in 2 - 4 Hz action potential bursting that projects to the ventral posterior thalamic relay nuclei. Drowsiness pattern detection involves elevated slow waves in the EEG maximal in Cz and Fz as well as alpha slowing. NeuroGuide does not use any regression methods to allegedly remove artifact such as ICA/PCA or Blind Source or unpublished methods like SARA that distort Phase and Coherence and other aspects of the Power Spectrum. Details and tutorials demonstrating how the ICA and regression methods distort Phase and Coherence are available at: https://www.appliedneuroscience.com/PDFs/Tutorial_Adulteration_Phase_Relations_when_using_ICA.pdf.

Split Half and Test Re-Test Reliability:

Split-Half (SH) reliability is the ratio of variance between the even and odd seconds of the time series of selected digital EEG (variance = sum of the square of the deviation of each time point from the mean of the time points). Examine the average reliability and the reliability of each channel as you increase the length of the sample and manually select different segments. Selection of artifact free EEG should have a reliability > 0.95 and a sample length of edited EEG > 60 seconds. Test Re-Test (TRT) reliability is the ratio of variance between the first half vs. the second half of the selected EEG segments (variance = sum of the square of the deviation of each time point from the mean of the time points). Test Re-Test reliability > 0.90 and a sample length of edited EEG > 60 seconds is commonly published in the scientific literature. Test Re-Test reliability is an excellent statistic to compare Brain state changes such as drowsiness as well as the consistency of a measure independent of changes in brain state.

Description of the NeuroGuide Normative Database:

The NeuroGuide normative database in versions 1.0 to 2.4.6 included a total of 678 carefully screened individual subjects ranging in age from 2 months to 82 years. NG 2.6.8 involved the addition of 49 adult subjects ranging in age from 18.3 years to 72.6 years resulting in a normative database of 727 subjects. The inclusion/exclusion criteria, demographics, neuropsychological tests, Gaussian distribution tests and cross-validation tests are described in several peer reviewed publications (Thatcher et al, 1983; 1987; 2003). Two year means were computed using a sliding average with 6 month overlap of subjects. This produced a stable and higher age resolution normative database with a total of 21 different age groups. The 21 age groups and age ranges and number of subjects per age group is shown in the bar graph in Appendix F figure 2 in the NeuroGuide Manual (click Help > NeuroGuide Help).

The individuals used to create the normative database met specific clinical standards of no history of neurological disorders, no history of behavioral disorders, performed at grade level in school, etc. Most of the subjects in the normative database were given extensive neuropsychological tests. Details of the normative database are published at: Thatcher, R.W., Walker, R.A. and Guidice, S. Human cerebral hemispheres develop at different rates and ages. *Science*, 236: 1110-1113, 1987 and Thatcher R.W., Biver, C.L., North, D., Curtin, R. and Walker, R.W. Quantitative EEG Normative Databases: Validation and Clinical Correlation. *Journal of Neurotherapy*, 2003, 7(3-4): 87-121. You can download a description of the normative database by going to www.appliedneuroscience.com and clicking on the webpage Articles & Links > Articles > Article #5.

Is there a normative database for different montages including bipolar montages?

Yes. The raw digital data from the same group of normal subjects is analyzed using different montages such as Average Reference, Laplacian current source density, a common reference based on all 19 channels of the 10/20 system and standard clinical bipolar montages (e.g., longitudinal, circular, transverse). Users can create any montage that they wish and there will be a normative reference database comparison available for both eyes closed and eyes open conditions.

Age range of the LORETA Current Density and Source Correlation Normative Databases

The LORETA current density and source correlation norms use the same subjects as are used for the surface EEG norms and the age range is 2 months to 82 years. The computational details of the LORETA current density norms are published at: Thatcher, R.W., North, D., Biver, C. EEG inverse solutions and parametric vs. non-parametric statistics of Low Resolution Electromagnetic Tomography (LORETA). Clin. EEG and Neuroscience, 36(1): 1-9, 2005 and Thatcher, R.W., North, D., Biver, C. Evaluation and Validity of a LORETA normative EEG database. Clin. EEG and Neuroscience, 2005, 36(2): 116-122. Copies of these publications are available to download from www.appliedneuroscience.com by clicking Articles & Links > Articles > Numbers 11 and 12. The computational details of the LORETA source correlation norms are in the NeuroGuide Manual, click Help > NeuroGuide Help > Appendix-G.

Implementation of LORETA measurement in NeuroGuide

The Key Institute's LORETA equations and the LORETA viewer (Pascual-Marqui et al, 1994; Pascual-Marqui, 1999) can be launched by a single mouse click in the NeuroGuide window. NeuroGuide exports frequency domain and time domain edits of 19 channel x 256 point digital EEG in microvolts (or μV^2) in the Lexicor electrode order as the standard input to the Key Institute T-Matrix. Rows are 256 microvolt time points and the columns are 19 channels at a sample rate of 128 thus producing 0.5 Hz resolution from 1 to 30 Hz. 1 Hz increments in the LORETA viewer are computed as the sum of adjacent 0.5 Hz bins and thus the 'Time Frame' control in the LORETA Viewer is frequency from 1 to 30 Hz. (see Pascual-Marqui RD, Michel CM, Lehmann D., 1994. Low resolution electromagnetic tomography: a new method for localizing electrical activity in the brain. International J. of Psychophysiology, 18:49-65. For computational details see: Pascual-Marqui. R.D., 1999. Review of Methods for Solving the EEG Inverse Problem. International J. of Bioelectromagnetism, 1(1): 75-86. Pascual-Margui, R.D., 2004. The Key Institute's free software and documentation was downloaded from www.unizh.ch/keyinst/NewLORETA/Software/Software.htm.)

Amplifier Matching is Necessary

This stems from the fact that amplifiers have different frequency gain characteristics. The matching of amplifiers to the NeuroGuide database amplifier was done by injecting microvolt calibration signals of different amplitudes and frequencies into the input of the respective EEG machines and then computing correction curves to exactly match the amplifier characteristics of the norms and discriminant functions. The units of comparison are in microvolts and a match within 3% is generally achieved. The NeuroGuide

research team double checked the amplifier match by computing FFT and digital spectral analyses on calibration signals used to acquire the norms with the calibration signals used to evaluate a given manufacturers amplifiers.

History of the Scientific Standards of QEEG Normative Databases

A review of the history of QEEG normative databases was published in Thatcher, R.W. and Lubar, J.F. History of the scientific standards of QEEG normative databases. In: Introduction to QEEG and Neurofeedback: Advanced Theory and Applications, T. Budzinsky, H. Budzinsky, J. Evans and A. Abarbanel (eds)., Academic Press, San Diego, CA, 2008. A copy of the publication can be downloaded at: https://www.appliedneuroscience.com/PDFs/History_of_QEEG_Databases.pdf.

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